

INTERSPINAL PROSTHESIS

The invention relates to an interspinal prosthesis of the introductory portion of claim 1, a counterpart thereto as well as to a multi-part interspinal prosthesis combined therefrom.

Such prostheses function as spacers for two adjacent vertebrae in the case of a defective disk, which would otherwise reduce the distance between the vertebrae. The stress on the facet joints is also relieved by the enlarged distance.

The W099/42051 discloses an interspinal prosthesis of this type, which includes a central piece, which is to be introduced into the interspinal space and from which a pair of ears arises cranially and caudially to the right and to the left of the central piece, in order to hold the central piece in the space between the spinous processes (processus spinosus) of two adjacent vertebrae after an implantation. A disadvantage of this known prosthesis is the fact that the latter is in one piece, which makes the implantation more difficult, so that it is necessary to remove the supraspinal ligament. The removal of this ligament has the disadvantage that the prosthesis is not held securely in the dorsal direction. For this reason, it is proposed in the WO99/42051 that the prosthesis be drilled through in the interspinal central piece, in order to pass a tape through the borehole, with which tape the prosthesis can be tied to the spinous processes of the adjacent vertebrae. This procedure is very time-consuming and complicated

The above discussion of the state of the art is given only to explain the environment of the invention and does not mean that the cited state of the art was also actually published or publicly known at the time of this application or its priority.

The invention is to provide a remedy here. It is therefore an object of the invention to provide an interspinal prosthesis, which can be implanted while

the supraspinal ligament is retained, so that the operation, as a whole, can be carried out more gently and the implant secured dorsally without additional means.

Pursuant to the invention, this objective is accomplished with a
5 multi-part, interspinal prosthesis, the individual parts of which may have different mechanical properties.

The inventive, interspinal prosthesis includes essentially a central
piece with a central axis, which can be introduced into the interspinal space, and
10 two processes, which arise at the outer ends and extend radially and diametrically to the central axis and can be introduced into the space between the spinous processes of two adjacent vertebrae. Furthermore, at the inner end of the central piece, averted from the spinous processes, there is an axial depression, which accommodates an essentially symmetrical counterpart to the prosthesis.

15 In a preferred embodiment, the central piece has coupling means, with which the counterpart can be fixed to the prosthesis. The coupling means therefore are constituted so that the positions of the processes at the prosthesis and the positions of the processes at the counterpart are determined relative to one
20 another when the counterpart is fixed in position. Preferably, the coupling means consist of a slide lock, which has a stop, so that, when the counterpart is attached to the prosthesis, the processes assume their desired positions at the prosthesis and the counterpart. Instead, of with a slide lock, the two parts can also be fixed to one another by a screwed or conical connection. In this case, the prosthesis and the
25 counterpart preferably have a twisting safeguard, so that the counterpart can be introduced only in a particular position into the axial depression at the prosthesis. A different configuration of the coupling means consist of at least one elastically deformable cam, which, after the prosthesis and counterpart are assembled, can be locked or snapped into position in the latter.

30 In a different, preferred embodiment of the inventive prosthesis, the coupling means comprise at least one elastically deformable cam, which, when the

prosthesis and counterpart are being assembled, can be deformed elastically and, after the prosthesis and counterpart are assembled, can be locked in position in a complementary depression.

5 A preferred further development consist therein that the cross-sectional planes, orthogonal to the central axis:

a) have an area of 50 to 300 mm² and preferably of 70 to two 250 mm² through the central piece at its narrowest site in the area of the inner end and

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b) an area of 70 to 500 mm² and preferably of 100 to 450 mm² through the processes.

15 Furthermore, the prosthesis is produced preferably from an elastic material, so that the central piece can be elastically deformed radially. A sufficient radial, elastic deformability can be achieved by producing the prosthesis from a plastic or by producing the central piece with cogs, which can be deformed radially and elastically.

20 The prosthesis may also be produced from an elastomer, silicone or a polymer from the polycarbonate family. It is, however, also possible to produce a prosthesis from a metallic material, if the elasticity of the prosthesis in the region of the central piece, which comes to rest in the interspinal space, can be realized by means of suitable mechanical devices.

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 In a different embodiment of the inventive prosthesis, the latter is constructed hollow, the hollow walls being collapsible and/or expandable by filling up the hollow spaces. The collapsible hollow walls have the advantage that, as a result, greater deformation of the prosthesis is made possible than would
30 be permitted by an elastic material.

In the region of the inner end, the outer surface of the central piece can be smooth or roughened. The adhesion of the bone to the prosthesis can be affected by the configuration of the outer surface, being promoted by a rough outer surface and made more difficult or even prevented by a smooth outer surface. The surface of the implant, which is in contact with the bone, can also be protected by embedding hydroxy apatite (HA).

In a preferred embodiment, the inventive counterpart comprises an inner end, an outer end as well as two processes, which arise at the outer end, also extend radially and diametrically and can be inserted in the space opposite the prosthesis and between the spinous processes of two adjacent vertebrae. Moreover, a peg, directed toward the inner end, is mounted at the counter part and can be introduced into the depression at the prosthesis. With that, an exact alignment of the prosthesis and the counterpart can be attained during the implantation.

Like the prosthesis, the counterpart can be fitted out with analogous, respectively complementary coupling means. Once again, these coupling means may comprise a slide lock, elastically deformable cams or a screwed or a conical connection. Likewise, an analogous, respectively complementary twisting safeguard is mounted at the counterpart.

The preferred embodiment of the inventive, interspinal prosthesis with a counterpart is distinguished owing to the fact, in the assembled state, it has a plane of symmetry orthogonal to the central axis, the processes of the interspinal prosthesis being at a distance of at least 2 mm and preferably of at least 3 mm from those of the counterpart, when viewed parallel to the central axis. The maximum distance of the processes of the interspinal prosthesis from those of the counterpart is 15 mm and preferably 12 mm.

The invention and further developments of the invention are explained in even greater detail in the following by means of partially diagrammatical representations of several examples. In the drawings,

- 5 Figure 1a shows a section through the preferred embodiment of the inventive, interspinal prosthesis with counterpart,
- Figure 1b shows a side view of the preferred embodiment of the embodiment of the inventive prosthesis with counterpart, shown in Figure 1a,
- 10 Figure 2 shows a section through a different embodiment of the inventive interspinal prosthesis with a counterpart,
- Figure 3 shows a section once again through a different embodiment of the
- 15 inventive interspinal prosthesis with a counterpart,
- Figure 4 shows a section through a further embodiment of the inventive interspinal prosthesis with a counterpart and
- 20 Figure 5 shows a view of a further embodiment of the inventive interspinal prosthesis with a counterpart.

In Figure 1, the interspinal prosthesis 1 with the counterpart 6 is shown in the assembled state. The central piece 2 of the prosthesis 1, with the

25 inner end 7 of the prosthesis 1, adjoins the counterpart 6. At the outer end 8 of the prosthesis 1, the two processes 3 are disposed perpendicularly to the central axis 4 and diametrically opposite to one another. In the embodiment shown here, the processes 3 are constructed as halves of an ellipsoid body. The also radial and diametrically opposite to one another processes 3 of the counterpart 6 are disposed

30 symmetrically to a plane, which is orthogonal to the central axis 4. Three radial cams 17, which are disposed symmetrically when viewed in the cross-section of the prosthesis 1 parallel to the central axis 4, protrude at the central piece 2 at the

inner end 7 of the prosthesis and engage complementary grooves 18 at the counterpart 6, function as twisting safeguard between the prosthesis 1 and the counterpart 6. Coaxially with the central axis 4, the central part 2 includes a depression 5, which penetrates from the inner end 7 into the prosthesis 1 up to a depth T. The counterpart 6 has a peg 16, which is constructed to be complementary to the depression 5 and accordingly, during the assembly of the prosthesis 1 and the counterpart 6, can be introduced into the depression 5. Furthermore, the prosthesis 1 comprises a fixing-in-position bolt 19 with a bolt head 26, which can be brought into contact with the outer end 8 of the prosthesis 1. The fixing-in-position bolt can be passed coaxially with the central axis 4 through the prosthesis 1 and locked by means of a slide lock 27 in the peg 16 of the counterpart 6, so that the prosthesis 1 can be locked detachably with the counterpart 6. A borehole 20, coaxial with the central axis 4, passes through the fixing-in-position bolt 19 and the counterpart 6, so that the prosthesis 1 and the counterpart 6 can be collapsed radially.

Figure 2 shows a further embodiment of the prosthesis with the counterpart 6 in the assembled state. The depression 5 passes through the prosthesis 1 coaxially from the inner end 7 up to the outer end 8. During the assembly of the prosthesis 1 and the counterpart 6, the peg 16 at the counterpart 6 is pushed into the through depression until the inner end 7 of the prosthesis 1 comes up against the processes 3 of the counterpart 6. Moreover, a borehole 20 is drilled through the counterpart 6 between the outer end 15 and the inner end 14. The coupling means 11 are constructed as a screwed connection, the screw 21 being passed through the depression 5 at the prosthesis 1 and through the borehole 20 at the counterpart 6 from the outer end 8 of the prosthesis 1 up to the outer end 15 of the counterpart 6 and bolted with a nut 22. In addition, the prosthesis 1 is provided with a hollow space 12, so that the walls 13 of the hollow space can be collapsed or, by filling the hollow space 12 with a filling material, expanded.

The embodiment, shown in Figure 3, differs from the embodiments described above in that the peg 16 at the counterpart 6 is passed completely

through the depression 5 at the prosthesis 1, so that the inner end 14 of the counterpart 6 aligns with the outer end 8 of the prosthesis 1 furthermore, the counterpart 6 has several boreholes 20, which are continuous from the inner end 14 to the outer end 15 and the axes of which extend parallel to the central axis 4.

- 5 The cerclage wires 23, by means of which the interspinal prosthesis 1 and the counterpart 6 are fixed in position, can be passed through these boreholes 21.

The embodiment, shown in Figure 4, differs from those shown in Figure 1 owing to the fact that the coupling means 11 comprise a locking bolt 28,
10 which can be passed through the borehole 20, which passes through the prosthesis 1 and the counterpart 6 coaxially with the central axis 4. The locking bolt 28, with its head 29, can be brought into contact with the outer end 15 of the counterpart 6 and has, at its tip, radially and elastically deformable cams 31, which, when the prosthesis 1 and the counterpart 6 are assembled, can be locked in an eccentric
15 relief 30, the diameter of which is larger than the diameter of the borehole 20, so that the prosthesis 1 and the counterpart 6 are held together. For introducing the locking bolt 28 into the borehole 20, the cams 31 can be compressed perpendicularly to the central axis 4 by means of axially disposed slots 32, so that the locking bolt 28 can be passed through the borehole 20, while, in the assembled
20 state, the cams 31 spring back elastically and latch into the eccentric relief 30 at the prosthesis 1. A hole is drilled through the locking bolt 28 coaxially with the central axis 4, so that a pin 25 can be passed through it, as a result of which a radial deflection of the cams 31 is prevented

25 In Figure 5, a further embodiment of the inventive prosthesis 1 with a counterpart 6 is shown. At the outer end 8 of the prosthesis 1 as well as at the outer end 15 of the counterpart 6, the processes 3 are mounted once again perpendicularly to the central axis 4 and diametrically opposite to one another, the processes 3 in this embodiment having a semicircular cross sectional surface
30 parallel to the central axis 4. The depression 5 passes through the prosthesis 1 from the inner end 7 to the outer end 8 coaxially with the central axis 4. In the depression 5, there is an internal thread 36 with a very large pitch. Adjoining the

inner end 14, the counterpart 6 once again has a peg 16, which has an external thread 33 that is complementary to the internal thread 36, so that the prosthesis 1 and the counterpart 6 can be fastened detachably to one another by means of this screwed connection. A first saw tooth-like system 34 is mounted at the
5 counterpart 6 between the peg 16 and the processes 3 and can be brought into engagement with a complementary second tooth system 35 at the inner end 7 of the prosthesis 1 during the assembly of the prosthesis 1 and the counterpart 6 so that, due to the asymmetric configuration of the saw tooth systems 34, 35, a safeguard is provided against the unintentional detachment of the prosthesis 1
10 from the counterpart 6.